# Lecture 7: Ultrasonically-induced Lorentz force imaging

Habib Ammari

Department of Mathematics, ETH Zürich

Habib Ammari

Mathematics of super-resolution biomedical imaging

- Mathematical and numerical framework for ultrasonically-induced Lorentz force electrical impedance tomography:
  - Ultrasonic vibration of a tissue in the presence of a static magnetic field → electrical current by the Lorentz force.
  - Current: depends nonlinearly on the conductivity distribution.
  - Imaging problem: reconstruct the conductivity distribution from measurements of the induced current.
  - Solve this nonlinear inverse problem:
    - Virtual potential: relate explicitly the current measurements to the conductivity distribution and the velocity of the ultrasonic pulse.
    - Wiener filtering of the measured data: reduce the problem to imaging the conductivity from an internal electric current density.
    - Optimal control approach.
    - Viscosity-type regularization method.



Example of the imaging device. A transducer is emitting ultrasound in a sample placed in a constant magnetic field. The induced electrical current is collected by two electrodes.



- Interaction between  $v(x, t)\xi$  and  $Be_3$ : induces Lorentz' force on the ions in  $\Omega \Rightarrow$  separation of charges  $\equiv$  source of current and potential:  $j_5(x, t) = \frac{B}{e^+}\sigma(x)v(x, t)\tau(\xi)$ ;  $\tau(\xi) = \xi \times e_3$ ;  $e^+$ : elementary charge.
- Voltage potential *u*:

$$\begin{cases} -\nabla \cdot (\sigma \nabla u) = \nabla \cdot j_S \text{ in } \Omega, \\ u = 0 \text{ on } \Gamma_1 \cup \Gamma_2, \ \frac{\partial u}{\partial \nu} = 0 \text{ on } \Gamma_0. \end{cases}$$

• Measured intensity:  $I(y,\xi) = \int_{\tau} \sigma \frac{\partial u}{\partial \nu}$ .

• Virtual potential:

$$U := F[\sigma] = \begin{cases} -\nabla \cdot (\sigma \nabla U) = 0 & \text{in } \Omega, \\ U = 0 & \text{on } \Gamma_1, \\ U = 1 & \text{on } \Gamma_2, \\ \partial_{\nu} U = 0 & \text{on } \Gamma_0. \end{cases}$$

- Assume that the support of v does not intersect the electrodes Γ<sub>1</sub> and Γ<sub>2</sub>.
- Integration by parts  $\Rightarrow$

$$-\int_{\Omega} \sigma \nabla u \cdot \nabla U + \int_{\Gamma_2} \sigma \frac{\partial u}{\partial \nu} = \int_{\Omega} j_S \cdot \nabla U \,.$$
$$I = \int_{\Omega} j_S \cdot \nabla U \,.$$

⇒

• Link between the measured intensity I and  $\sigma$ :

$$I=\frac{B}{e^+}\int_{\Omega}v(x,t)\sigma(x)\nabla U(x)dx\cdot\tau\,.$$

- v depends on y,  $\xi$ , and t, so does I.
- Define the measurement function:

$$M(y,\xi,z) = \int_{\Omega} v(x,z/c)\sigma(x)\nabla U(x)dx \cdot \tau(\xi)$$

for any  $y \in \mathbb{R}^3$ ,  $\xi \in S$  and z > 0.

 Assume the knowledge of this function in a certain subset of ℝ<sup>3</sup> × S × ℝ<sup>+</sup> denoted by Y × 𝔅 × (0, z<sub>max</sub>).

- Construction of the virtual current: Obtain σ∇U from M ← separate v from M.
- Ultrasound pulse:

$$\begin{aligned} \mathbf{v}(x,t) &= \mathbf{w}(z-ct) \ \mathbf{A}(z,|r|);\\ z &= (x-y) \cdot \xi \text{ and } r = x-y-z\xi \ \in \Upsilon_{\xi} := \{\zeta \in \mathbb{R}^3 \ : \ \zeta \cdot \xi = 0\}. \end{aligned}$$

$$\bullet \text{ For any } z \in (0, z_{max}), \end{aligned}$$

$$\begin{split} M(y,\xi,z) &= \int_{\mathbb{R}} \int_{\Upsilon_{\xi}} w(z-z') (\sigma \nabla U) (y+z'\xi+r) A(z',|r|) dr dz' \cdot \tau(\xi) \\ &= \int_{\mathbb{R}} w(z-z') \int_{\Upsilon_{\xi}} (\sigma \nabla U) (y+z'\xi+r) A(z',|r|) dr dz' \cdot \tau(\xi) \\ &= (W \star \Phi_{y,\xi}) (z) \cdot \tau(\xi) \,, \end{split}$$

W(z) = w(-z); \*: convolution product;

$$\Phi_{y,\xi}(z) = \int_{\Upsilon_{\xi}} \sigma(y+z\xi+r)A(z,|r|)\nabla U(y+z\xi+r)dr$$

- Deconvolution:
  - Recover Φ<sub>y,ξ</sub> from the measurements M(y, ξ, ·) in the presence of noise.
  - Wiener-type filter.
  - Assume that the signal M(y, ξ, ·) is perturbed by a random white noise:

$$\widetilde{M}(y,\xi,z) = M(y,\xi,z) + \mu(z),$$

 $\mu$ : white Gaussian noise with variance  $\nu^2$  s.t.

$$\mathbb{E}[\mu(z)\mu(z')] = \nu^2 \delta_0(z-z')$$

and

$$\mathbb{E}[\mathcal{F}(\mu)(k)\overline{\mathcal{F}(\mu)(k')}] = 
u^2 \delta_0(k-k')$$

where

$$\mathcal{F}[\mu](k) = rac{1}{\sqrt{2\pi}}\int \mu(z)e^{-ikz}dz$$
 .

$$\widetilde{M}_{\!\scriptscriptstyle \mathcal{Y},\xi}(z) = \left( W \star \Psi_{\scriptscriptstyle \mathcal{Y},\xi} 
ight)(z) + \mu(z) \, ,$$

 $\Psi_{y,\xi}(z) = \Phi_{y,\xi}(z) \cdot \tau(\xi).$ 

- S(Ψ<sub>y,ξ</sub>) = ∫<sub>ℝ</sub> |F(Ψ<sub>y,ξ</sub>)(k)|<sup>2</sup>dk: spectral density of Ψ<sub>y,ξ</sub>; F: Fourier transform.
- Wiener deconvolution filter in the frequency domain:

$$\widehat{L}(k) = rac{\overline{\mathcal{F}(W)}(k)}{|\mathcal{F}(W)|^2(k) + rac{
u^2}{S(\Psi_{y,\xi})}}$$

- Quotient  $S(\Psi_{y,\xi})/\nu^2$ : signal-to-noise ratio.
- A priori estimate of the signal-to-noise ratio.
- Recover  $\Psi_{y,\xi}$  up to a small error by

$$\widetilde{\Psi}_{y,\xi} = \mathcal{F}^{-1}\left(\mathcal{F}(\widetilde{M})\widehat{L}\right) \,.$$

- Wiener deconvolution filter: recover D(x) = (σ∇U)(x) from measured intensities I(y, ξ).
- Recover  $\sigma$  from  $D = \sigma \nabla U$ .
- Optimal control algorithm.

• For 
$$a < b$$
,  $L^{\infty}_{a,b}(\Omega) := \{f \in L^{\infty}(\Omega) : a < f < b\}$ ; Define  $\mathcal{F} : L^{\infty}_{\underline{\sigma},\overline{\sigma}}(\Omega) \to H^{1}(\Omega)$  by

$$\mathcal{F}[\sigma] = \mathcal{U} : \begin{cases} \nabla \cdot (\sigma \nabla \mathcal{U}) = 0 & \text{ in } \Omega \,, \\ \mathcal{U} = 0 & \text{ on } \Gamma_1 \,, \\ \mathcal{U} = 1 & \text{ on } \Gamma_2 \,, \\ \frac{\partial \mathcal{U}}{\partial \nu} = 0 & \text{ on } \Gamma_0 \,. \end{cases}$$

*dF*: Fréchet derivative of *F*. For any *σ* ∈ *L*<sup>∞</sup><sub><u>σ</u>,<u>σ</u></sub>(Ω) and *h* ∈ *L*<sup>∞</sup>(Ω) s.t. *σ* + *h* ∈ *L*<sup>∞</sup><sub><u>σ</u>,<u>σ</u></sub>(Ω),

$$d\mathcal{F}[\sigma](h) = \mathbf{v}: \begin{cases} \nabla \cdot (\sigma \nabla \mathbf{v}) = -\nabla \cdot (h \nabla \mathcal{F}[\sigma]) & \text{in } \Omega, \\ \mathbf{v} = 0 & \text{on } \Gamma_1 \cup \Gamma_2, \\ \frac{\partial \mathbf{v}}{\partial \nu} = 0 & \text{on } \Gamma_0. \end{cases}$$

御 と く ヨ と く ヨ と …

• Proof: 
$$w = \mathcal{F}[\sigma + h] - \mathcal{F}[\sigma] - v$$
 satisfies  
 $\nabla \cdot (\sigma \nabla w) = -\nabla \cdot (h \nabla (\mathcal{F}[\sigma + h] - \mathcal{F}[\sigma]))$ 

with the same boundary conditions as v.

• Elliptic global control:

$$\begin{split} \|\nabla w\|_{L^{2}(\Omega)} &\leq \frac{1}{\sigma} \|h\|_{L^{\infty}(\Omega)} \|\nabla (\mathcal{F}[\sigma+h] - \mathcal{F}[\sigma])\|_{L^{2}(\Omega)} \ . \end{split}$$

$$\bullet \ \nabla \cdot (\sigma \nabla (\mathcal{F}[\sigma+h] - \mathcal{F}[\sigma])) = -\nabla \cdot (h \nabla \mathcal{F}[\sigma+h]), \Rightarrow$$

$$\left\| 
abla (\mathcal{F}[\sigma+h]-\mathcal{F}[\sigma]) 
ight\|_{L^2(\Omega)} \leq rac{1}{\sqrt{\sigma}} \left\| h 
ight\|_{L^\infty(\Omega)} \left\| 
abla \mathcal{F}[\sigma+h] 
ight\|_{L^2(\Omega)} \,.$$

•  $\Rightarrow$  There is a positive constant *C* depending only on  $\Omega$  s.t.

$$\|\nabla \mathcal{F}[\sigma+h]\|_{L^2(\Omega)} \leq C\sqrt{\frac{\overline{\sigma}}{\underline{\sigma}}}.$$

• =

$$\|\nabla w\|_{L^{2}(\Omega)} \leq C \frac{\sqrt{\overline{\sigma}}}{\underline{\sigma}^{2}} \|h\|_{L^{\infty}(\Omega)}^{2}$$

- Minimization of the functional:  $J[\sigma] = \frac{1}{2} \int_{\Omega} |\sigma \nabla \mathcal{F}[\sigma] D|^2$ .
- Gradient of J: For any  $\sigma \in L^{\infty}_{\sigma,\overline{\sigma}}(\Omega)$  and  $h \in L^{\infty}(\Omega)$  s.t.  $\sigma + h \in L^{\infty}_{\sigma,\overline{\sigma}}(\Omega)$ ,

$$dJ[\sigma](h) = -\int_{\Omega} h\Big((\sigma \nabla \mathcal{F}[\sigma] - D - \nabla p) \cdot \nabla \mathcal{F}[\sigma]\Big);$$

*p*: solution to the adjoint problem:

$$\begin{cases} \nabla \cdot (\sigma \nabla p) = \nabla \cdot (\sigma^2 \nabla \mathcal{F}[\sigma] - \sigma D) & \text{in } \Omega, \\ p = 0 & \text{on } \Gamma_1 \cup \Gamma_2, \\ \frac{\partial p}{\partial \nu} = 0 & \text{on } \Gamma_0. \end{cases}$$

• Proof  $\mathcal{F}$ : Fréchet differentiable  $\Rightarrow$  *J*: Fréchet differentiable. For  $\sigma \in L^{\infty}_{\sigma,\overline{\sigma}}(\Omega)$  and  $h \in L^{\infty}(\Omega)$  s.t.  $\sigma + h \in L^{\infty}_{\sigma,\overline{\sigma}}(\Omega)$ ,

$$dJ[\sigma](h) = \int_{\Omega} (\sigma \nabla \mathcal{F}[\sigma] - D) \cdot (h \nabla \mathcal{F}[\sigma] + \sigma \nabla d\mathcal{F}[\sigma](h)).$$

• 
$$\Rightarrow$$
  

$$\int_{\Omega} \sigma \nabla p \cdot \nabla d\mathcal{F}[\sigma](h) = \int_{\Omega} (\sigma^{2} \nabla \mathcal{F}[\sigma] - \sigma D) \cdot \nabla d\mathcal{F}[\sigma](h) \cdot \int_{\Omega} \sigma \nabla p \cdot \nabla d\mathcal{F}[\sigma](h) = -\int_{\Omega} h \nabla \mathcal{F}[\sigma] \cdot \nabla p ,$$
•  $\Rightarrow$   

$$dJ[\sigma](h) = \int_{\Omega} h(\sigma \nabla \mathcal{F}[\sigma] - D - \nabla p) \cdot \nabla \mathcal{F}[\sigma] .$$

-∢ ⊒ ▶

• Optimal control algorithm:

• 
$$\min_{\sigma} \int_{\Omega} |\sigma \nabla F[\sigma] - D|^2 + \text{regularization term (a prior)}$$
:

 σ: smooth variations out of the discontinuity set ⇒ regularized functional:

$$J_{\varepsilon}[\sigma] = \frac{1}{2} \int_{\Omega} \left| \sigma \nabla \mathcal{F}[\sigma] - D \right|^{2} + \varepsilon \left| \sigma \right|_{\mathcal{TV}(\Omega)},$$

 $\varepsilon >$  0: regularization parameter.

• Nonconvexity (numerically); high sensitivity to noise.

#### Direct method

• Assume  $U(x) = x_2 \Gamma_0 \Rightarrow U$ : solution of the transport equation:

$$\begin{cases} D^{\perp} \cdot \nabla U = 0 & \text{in } \Omega, \\ U = x_2 & \text{on } \partial \Omega. \end{cases}$$

• If transport equation: well posed and can be solved  $\Rightarrow$  we can reconstruct the virtual potential  $U \Rightarrow$ 

$$\frac{1}{\sigma} = \frac{D \cdot \nabla U}{|D|^2} \,.$$

- First-order equation: really tricky.
- Existence and uniqueness challenging if *F*: discontinuous.
- Characteristic method: unstable.

#### Direct method

• Viscosity-type regularization method:

$$\begin{cases} \nabla \cdot (\varepsilon I + (D^{\perp}(D^{\perp})^{T}) \nabla U_{\varepsilon} = 0 & \text{in } \Omega, \\ U_{\varepsilon} = x_{2} & \text{on } \partial \Omega. \end{cases}$$

Reconstructed image:

$$\frac{1}{\sigma_{\varepsilon}} := \frac{D \cdot \nabla U_{\varepsilon}}{|D|^2} \to \frac{1}{\sigma_*} \text{in } L^2$$

as the viscosity parameter  $\varepsilon \rightarrow 0$ ;  $\sigma_*$ : true conductivity.

- $(U_{\eta} U)_{\varepsilon > 0}$  converges strongly to zero in  $H_0^1(\Omega)$ .
- Proof:
  - $F := D^{\perp}$ .
  - $(U_{\varepsilon} U)_{\varepsilon > 0} \rightarrow 0$  weakly.
  - For any arepsilon>0,  $ilde{U}_arepsilon:=U_arepsilon-U\in H^1_0(\Omega)$  and satisfies

$$abla \cdot \left[ \left( \varepsilon I + FF^T \right) \nabla \tilde{U}_{\varepsilon} \right] = -\varepsilon \Delta U \quad \text{in } \Omega.$$

• Integration by parts  $\Rightarrow$ 

$$\begin{split} \varepsilon \int_{\Omega} |\nabla \tilde{U}_{\varepsilon}|^{2} + \int_{\Omega} |F \cdot \nabla \tilde{U}_{\varepsilon}|^{2} &= -\varepsilon \int_{\Omega} \nabla U \cdot \nabla \tilde{U}_{\varepsilon}. \\ \bullet \Rightarrow \\ \left\| \tilde{U}_{\varepsilon} \right\|_{H_{0}^{1}(\Omega)}^{2} &\leq \int_{\Omega} |\nabla U \cdot \nabla \tilde{U}_{\varepsilon}| \leq \| U \|_{H^{1}(\Omega)} \left\| \tilde{U}_{\varepsilon} \right\|_{H_{0}^{1}(\Omega)} \end{split}$$

.

• 
$$\Rightarrow \left\| \tilde{U}_{\varepsilon} \right\|_{H^{1}_{0}(\Omega)} \leq \left\| U \right\|_{H^{1}(\Omega)}$$

(Ũ<sub>ε</sub>)<sub>ε>0</sub>: bounded in H<sup>1</sup><sub>0</sub>(Ω); by Banach-Alaoglu's theorem ⇒ extract a subsequence which converges weakly to U<sup>\*</sup> in H<sup>1</sup><sub>0</sub>(Ω).

$$\int_{\Omega} \left( F \cdot \nabla \tilde{U}_{\varepsilon} \right) \left( F \cdot \nabla U^* \right) = -\varepsilon \int_{\Omega} \nabla U \cdot \nabla U^* - \varepsilon \int_{\Omega} \nabla \tilde{U}_{\varepsilon} \cdot \nabla U^* \,.$$

•  $\varepsilon \to 0$ ,  $\|F \cdot \nabla U^*\|_{L^2(\Omega)} = 0$ .  $\Rightarrow U^*$ : solution the transport equation:

$$\begin{cases} F \cdot \nabla U^* = 0 & \text{ in } \Omega \,, \\ U^* = 0 & \text{ on } \partial \Omega \,. \end{cases}$$

- Uniqueness of a solution  $\Rightarrow U^* = 0$  in  $\Omega$ .
- $U^*$ : independent of the subsequence  $\Rightarrow$  convergence holds for  $\tilde{U}_{\varepsilon}$ .

• Strong convergence:

• 
$$\begin{split} & \int_{\Omega} |\nabla \tilde{U}_{\varepsilon}|^{2} \leq -\int_{\Omega} \nabla U \cdot \nabla \tilde{U}_{\varepsilon} \, . \\ \bullet \quad \tilde{U}_{\varepsilon} \rightharpoonup 0 \text{ in } H^{1}_{0}(\Omega) \Rightarrow \left\| \tilde{U}_{\varepsilon} \right\|_{H^{1}_{0}(\Omega)} \to 0. \\ & \left\| \frac{1}{\sigma_{\varepsilon}} = \frac{D \cdot \nabla U_{\varepsilon}}{|D|^{2}} \\ \end{split}$$
strongly converges to  $\frac{1}{\sigma_{*}}$  in  $L^{2}(\Omega)$ .

Mathematics of super-resolution biomedical imaging

・日本 ・日本 ・日本



Mathematics of super-resolution biomedical imaging

#### Habib Ammari

